

Analysis of liposome model systems by time-of-flight secondary ion mass spectrometry

Downloaded from: https://research.chalmers.se, 2025-07-02 11:03 UTC

Citation for the original published paper (version of record):

Lovric, J., Keighron, J., Angerer, T. et al (2014). Analysis of liposome model systems by time-of-flight secondary ion mass spectrometry. Surface and Interface Analysis, 46(S1): 74-78. http://dx.doi.org/10.1002/sia.5623

N.B. When citing this work, cite the original published paper.

research.chalmers.se offers the possibility of retrieving research publications produced at Chalmers University of Technology. It covers all kind of research output: articles, dissertations, conference papers, reports etc. since 2004. research.chalmers.se is administrated and maintained by Chalmers Library



Optimizing Interface Conductivity in Electronics



E*♥*IDENT

OLYMPUS

WILEY

The latest eBook from Advanced Optical Metrology. Download for free.

Surface roughness is a key parameter for judging the performance of a given material's surface quality for its electronic application. A powerful tool to measure surface roughness is 3D laser scanning confocal microscopy (LSM), which will allow you to assess roughness and compare production and finishing methods, and improve these methods based on mathematical models.

Focus on creating high-conductivity electronic devices with minimal power loss using laser scanning microscopy is an effective tool to discern a variety of roughness parameters.



Received: 2 June 2014

(wileyonlinelibrary.com) DOI 10.1002/sia.5623

Analysis of liposome model systems by timeof-flight secondary ion mass spectrometry

Jelena Lovrić,^a Jacqueline D. Keighron,^a Tina B. Angerer,^b Xianchan Li,^a Per Malmberg,^a John S. Fletcher^b and Andrew G. Ewing^{a,b}*

Time-of-flight secondary ion mass spectrometry (ToF-SIMS) is an important technique for studying chemical composition of micrometer scale objects because of its high spatial resolution imaging capabilities and chemical specificity. In this work, we focus on the application of ToF-SIMS to gain insight into the chemistry of micrometer size liposomes as a potential model for neurotransmitter vesicles. Two models of giant liposomes were analyzed: histamine and aqueous two-phase system-containing liposomes. Characterization of the internal structure of single fixed liposomes was carried out both with the Bi_3^+ and C_{60}^+ ion sources. The depth profiling capability of ToF-SIMS was used to investigate the liposome interior. Copyright © 2014 John Wiley & Sons, Ltd.

Additional supporting information may be found in the online version of this article at the publisher's web-site.

Accepted: 23 June 2014

Keywords: liposome; aqueous two-phase system; histamine; ToF-SIMS; depth profile analysis; imaging

Introduction

Liposomes are phospholipid bilayer vesicles, which resemble cellular organelles. Because of their biodegradable and biocompatible nature, they have found applications in a wide range of fields such as drug delivery, gene therapy, cosmetics, and food technology.^[1-3]

ToF-SIMS is a prominent analytical technique to study the chemistry in a vast spectrum of biological samples such as tissues,^[4–6] cells,^[7,8] sub-cellular compartments,^[9] as well as organisms,^[10,11] pharmacological systems,^[12] drug delivery,^[13] and metabolite pathways.^[14] The capability for three-dimensional imaging of organics is achieved by employing cluster ion sources such as $C_{60}^{[15]}$ and gas cluster ion beams.^[16–18]

In this paper, we have investigated the interior of liposomes as a model system for carriers of variety of chemicals.^[1–3,19] Two separate systems have been employed: (1) histamine encapsulating liposomes^[19,20] representing one compartment and (2) liposomes containing an aqueous two-phase system (ATPS) composed of dextran and poly(ethylene glycol)^[21] as a two-compartment liposome model. Mass spectrometric imaging and depth profiling were carried out with single beam C_{60}^+ on a J105 – *3D Chemical Imager* (lonoptika Ltd, UK)^[7] and in dual beam mode using C_{60}^{3+} for etching and Bi₃⁺ for analysis on a TOF.SIMS V instrument. The former instrument allowed us to analyze the histamine peak relative to silicon, whereas the latter one allowed us to acquire high-spatial resolution images of lipid membrane and poly(ethylene glycol) in the liposome model.

Experimental

Materials

1,2-Dipalmitoyl-*sn*-glycero-3-phosphocholine (DPPC), cholesterol (ovine wool), $l-\alpha$ -phosphatidylcholine (Soy PC), 1,2-dipalmitoyl-*sn*-glycero-3-phospho-(1'*-rac*-glycerol) (sodium salt) (DPPG) and Avanti

Mini-Extruder were purchased from Avanti Polar Lipids, Alabama. Histamine dihydrochloride, poly(ethylene glycol) (PEG, MW 8000), dextran (from Leuconostoc spp. MW 450 000–600 000) were obtained from Sigma-Aldrich, Sweden. Whatman nucleopore tracketched polycarbonate membranes, pore size $5 \,\mu$ m and Thermo Scientific Slide-A-Lyzer Dialysis Cassettes (10 K MWCO) were purchased from Fisher Scientific, Sweden.

Sample preparation

1. One-compartment liposome model (histamine-containing giant liposomes).^[19] A chloroform solution of lipids containing a 9:1 molar ratio of DPPC to cholesterol, total lipid of 12.3 mg/mL, was vacuum desiccated for 2 h. The lipid cake was rehydrated with 5 mL 0.5 M histamine dihydrochloride solution for 30 min at room temperature. Liposomes were then exposed to five freeze-thaw cycles in a freezer (-80 °C) and warm water bath. The liposomal suspension was extruded over the polycarbonate membrane 21 times at 70 °C. Excess histamine dihydrochloride was excluded by dialysis with MQ water for 2 h. The liposome suspension was then diluted twofold with MQ water, placed onto a clean silicon wafer, and dried under atmospheric pressure at room temperature. The liposomes were visualized under transmitted light using differential interference contrast (DIC) microscopy with an Olympus IX-71 microscope showing they had diameters between 3 and 5 μ m.

^{*} Correspondence to: A. G. Ewing, Department of Chemical and Biological Engineering, Chalmers University of Technology, SE-412 96 Gothenburg, Sweden. E-mail: andrewe@chalmers.se

a Department of Chemical and Biological Engineering, Chalmers University of Technology, SE-412 96 Gothenburg, Sweden

b Department of Chemistry and Molecular Biology, University of Gothenburg, SE-412 96 Gothenburg, Sweden

2. Two-compartment liposome model (ATPS-containing giant liposomes)^[21] were prepared by mixing Soy PC and DPPG at molar ratio 9:1 (5 mg/mL; total lipids). The lipid mixture was evaporated for 3 h under vacuum before hydration for 12 h at 40 °C with 2 mL 4% PEG/4% dextran. The liposome suspension was phase separated at 4 °C, and liposomes were collected through the PEG-enriched phase from the interface of two-phase-separated polymers (Fig. 3b). Liposome size was determined visually (10–30 μ m in diameter). Sample freezing and freeze-fracturing was carried out as previously described.^[22]

TOF-SIMS analysis

ToF-SIMS analysis was performed on a TOF.SIMS V instrument (ION-TOF GmbH, Germany) and a J105 – *3D Chemical Imager*.

TOF.SIMS V analysis

A ${\rm Bi_n}^{q+}$ LMIG was employed for imaging and a ${\rm C_{60}}^{q+}$ ion source for sample sputtering. Data were recorded in positive ion mode with extraction voltage 2000 V, and charge compensation was performed by flooding with low-energy electrons. Spectra were acquired using ${\rm Bi_3}^+$ primary ions (25 keV) in burst alignment imaging mode^[23] with a 100-ns primary ion beam pulse width.



Figure 1. One-compartment liposome model (histamine-containing giant liposomes) imaged with a J105 – *3D Chemical Imager*. Data shown are from the second layer of analysis after the first image acquisition when the surface of the sample was removed exposing the liposome interior. Acquisition time: $22 \min/layer$; pixel resolution of 500 nm/pixel; analysis area: $130 \times 130 \mu m^2$; 256×256 pixel images were acquired with a primary ion dose density of $2.42 \times 10^{13} ions-cm^{-2}/layer$. (a) An overlay of PC (*m/z* 184.1; red), silicon (*m/z* 111.9; blue), and histamine (*m/z* 112.1; green). (b) Ion image of PC at *m/z* 184.1. (c) Ion image of silicon at *m/z* 111.9. (d) Ion image of histamine at *m/z* 112.1. (e) Mass spectrum from image showing the two peaks at *m/z* 112.

Depth profile analysis was carried out in burst alignment mode^[23] with Bi_3^+ primary ions (pulsed current measurement with current value of 0.25 pA) for imaging and C_{60}^{3+} in direct current mode (30 keV, current 0.2 nA) for sputtering.

J105 – 3D Chemical Imager analysis

A 40-keV C_{60}^+ primary ion beam in the positive ion mode was used. The instrument employs a quasi-continuous primary ion beam to produce a stream of secondary ions. The secondary ions are compressed using a linear buncher to produce a tight packet of ions at the entrance to a quadratic field reflectron. The mass resolution is dependent on the tuning of the buncher and not the ion formation process. An extraction voltage of 1000 V, over an extraction gap of approximately 7 mm, was used. Electron flooding was not employed.

Results and discussion

In order to establish the most suitable methodology for mass spectrometric imaging of the liposomal interior, two different samples were prepared and analyzed by ToF-SIMS.

Histamine-encapsulated giant liposomes were designed as our first liposome model to allow imaging of the chemical messenger, histamine, inside an individual liposome with the J105. For experimental simplicity, we have studied dry liposomes at room temperature. Figures 1a–1d represent molecular chemical maps of dry liposomes acquired by analyzing whole liposomes. A series of images (layers) were acquired with the spectral dose density of 2.42×10^{13} ions-cm⁻²/layer. The total dose density to completely remove the liposome was 1.21×10^{14} ions-cm⁻² (five layers). The lipid head group, phosphatidylcholine (PC) with *m/z* 184, is observed showing the lipid membrane and the histamine fragment with *m/z* 112.1 inside the liposome that is shown clearly as a color overlay (Fig. 1a). This evidence suggests that it is possible to

10969918, 2014, S1, Downloaded from https://analyticals

onlinelibrary.wiley.com/doi/10.1002/sia.5623 by Chalmers University Of Technology, Wiley Online Library on [08/08/2023]. See the Terms

and Conditions

(https://onli

on Wiley Online Library

for rules

of use; OA articles are governed by the applicable Creative Comm

image liposomal content. A typical mass spectrum for the dry histamine-filled liposomes is reported in Fig. 1e. At the nominal mass m/z 112, there are two different peaks that, when imaged, localize at two different locations (Fig. 1c and 1d). From the calculation of exact masses, the inorganic peak m/z 111.9 is assigned to the silicon (Fig. 1c), which is present as the substrate around the liposomes, whereas the peak at m/z 112.1 is localized in the liposomes and represents the histamine fragment (Fig. 1d). Thus, the mass spectrum with two well-resolved masses 0.2 amu apart allows us to state that we are able to image this type of sample with good mass and spatial resolution.

We next introduced a more complex two-compartment liposomal sample containing an internal morphology. For this purpose, liposomes containing an ATPS made of PEG and dextran polymers have been used. Figure 2a shows the DIC image of such a liposome where polymer phases are distinguishable. The dextran-rich phase located in the center of the liposome appears to project out of the image plane because of higher concentration of optically active dextran. Further, the sample was freezefractured to provide a frozen-hydrated state in order to avoid redistribution of the lipid membrane and other components.^[24] The mass spectrometric images were acquired with the TOF.SIMS V with accumulated dose density of $3.21 \times 10^{13} \text{Bi}_3^+/\text{cm}^2$. Based on ToF-SIMS analysis of polymer standards, it was determined that the most abundant fragments for PEG were fragments with m/z 45 and 87 while the most intense dextran fragment was m/z 127. The assigned fragments for PC were m/z 86 and 184. The ion images of the PC and PEG fragments are shown in Figs 2d–2f, and a color overlay of m/z 86 and 87 fragments in Fig. 2b. A morphological pattern similar to that shown in a DIC microscopic image of a similar ATPS-containing liposome (Fig. 2a) is also observed in the ion images (Fig. 2b-2f). Both PC ion fragments (m/z 86 and 184) originate from the lipid membrane. In biological systems, only fragment m/z 224.1 is specific for PC



Figure 2. Two-compartment liposome model (ATPS-containing giant liposome) imaged with (a) DIC and (b–f) the TOF.SIMS V. Acquisition time: 360.45 s; FoV: $42 \times 42 \mu m^2$; pixel resolution: 195 nm/pixel. Details: (b) An overlay of PC (m/z 86; red) and PEG (m/z 87; green). (c) Total ion image. (d) Ion image of PC at m/z 184. (e) Ion image of PC at m/z 86. (f) Ion image of PEG at m/z 87. All images are binned (4 pixels).



Figure 3. Depth profile of two-compartment liposome model across the ATPS-containing giant liposome. (a) ToF-SIMS sputter depth profile acquired with the TOF.SIMS V. Acquisition time: 97.16 s; fluence: 3.33×10^{13} Bi₃^{+/}cm²; FoV (Bi₃⁺): $105 \times 105 \,\mu\text{m}^2$; FoV (C₆₀³⁺): $200 \times 200 \,\mu\text{m}^2$. (b) Schematic of liposome embedded in frozen PEG-enriched phase. (c) Depth profile was reconstructed from the specific region of interest.

and is distinguishable from sphingomyelin.^[4] In our model system, the assigned fragments for PC, m/z 86 and 184, were used to determine lipid membrane, as in the liposome preparation, we do not employ sphingomyelin, and we are interested in the liposomal content. To apply SIMS imaging to probe the membranes of neurotransmitter vesicles, only fragment m/z 224.1 is truly specific for PC. Signal originating from PEG with m/z 87 is more intense in the central part of the imaged feature (Fig. 2f and Fig. S1) suggesting that PEG was localized in a specific portion of the liposome interior. Comparison to the total ion signal indicates that this localization is due to chemical changes and not the morphology of the liposome. Furthermore, the freeze-fractured frozen-hydrated ATPS liposome was depth profiled using the TOF. SIMS V where analysis was performed using Bi₃⁺ and for etching C_{60}^{3+} ions were used. Several characteristic fragments were monitored while sputtering through the sample (dextran m/z 127, PEG m/z 45, and PC m/z 184). Figure 3 shows the depth profiling data across the entire liposome, and a few features are noteworthy. Considering the accumulated etch dose density of 1.87×10^{14} ions-cm⁻², sample nature, and C₆₀³⁺ organic depth profiling data obtained by Shard et al., [25] it is estimated that the erosion depth was approximately 350 nm. According to the previously reported studies, the lipid bilayer thickness is approximated to be 5 nm.^[26,27] Our depth profiling data (Fig. 3a) shows that PEG signal has the highest intensity in the beginning of profile acquisition showing that liposomes were embedded in the PEG-enriched environment. Further, a sharp rise in the signal for the PC fragment at m/z 184 showed the location of the lipid membrane, and a rise in the m/z 45 peak was related to the PEG phase within the liposome, continued etching then revealed the dextran core. These data suggest that the etching occurred in the fraction of liposomal volume where the dextran core is close to the lipid membrane (Fig. 2a and 3b). Thus, depth profiling allowed us to probe into a liposome and to determine the lateral morphology of the liposome interior with chemical specificity.

Conclusion

We have shown that the ToF-SIMS technique is capable of generating 2D images and depth profiles of the inner morphology of micrometer-sized liposomes allowing us to determine the microcompartmentation. Acquisition of 2D images of onecompartment liposome model demonstrates that we can laterally probe the interior composition of the liposome, whereas the experiments to depth profile of the more complex two-compartment liposomes show that we can distinguish internal morphology. Therefore, we suggest the application of ToF-SIMS for imaging the compartments inside liposomal models, and our future work will focus on imaging the distribution patterns of neurotransmitters in and laterally across cellular vesicles with ToF-SIMS.

Acknowledgements

This research was funded by the Joint Chalmers-GU Center for Bioanalytical Chemistry, the Swedish Research Council (VR), European Research Council (ERC), Wallenberg Foundation, and the USA National Institutes of Health (NIH). The SIMS experiments were conducted at the National Center for Imaging Mass Spectrometry (NCIMS). The authors kindly acknowledge Masoumeh Dowlatshahipour for providing help in sample preparation.

References

- [1] M. R. Mozafari, *Methods Mol. Biol.* **2010**, *605*, 29.
- [2] A. Moscho, O. Orwar, D. T. Chiu, B. P. Modi, R. N. Zare, Proc. Natl. Acad. Sci. U. S. A. **1996**, 93, 11443.

- [3] T. Lian, R. J. Y. Ho, J. Pharm. Sci. 2001, 90, 667.
- [4] N. Tahallah, A. Brunelle, S. De La Porte, O. Laprévote, J. Lipid Res. 2008, 49, 438.
- [5] S. Ayciriex, D. Touboul, A. Brunelle, O. Laprévote, Clin. Lipidol. 2011, 6, 437.
- [6] D. Debois, A. Brunelle, O. Laprévote, Int. J. Mass Spectrom. 2007, 260, 115.
- [7] J. S. Fletcher, J. C. Vickerman, Anal. Chem. 2013, 85, 610.
- [8] E. B. Monroe, J. C. Jurchen, J. Lee, S. S. Rubakhin, J. V. Sweedler, J. Am. Chem. Soc. 2005, 127, 12152.
- [9] S. Rabbani, J. S. Fletcher, N. P. Lockyer, J. C. Vickerman, Surf. Interface Anal. 2011, 43, 380.
- [10] S. G. Ostrowski, C. T. Van Bell, N. Winograd, A. G. Ewing, *Science*, 2004, 305, 71.
- [11] M. E. Kurczy, P. D. Piehowski, C. T. Van Bell, M. L. Heien, N. Winograd, A. G. Ewing, Proc. Natl. Acad. Sci. U. S. A. 2010, 107, 2751.
- [12] C. T. Dollery, Clin. Pharmacol. Ther. (N. Y., NY, U. S.) 2013, 93, 263.
- [13] P. Fragu, E. Kahn, Microsc. Res. Tech. 1997, 36, 296.
- [14] P. Malmberg, E. Jennische, D. Nilsson, H. Nygren, Anal. Bioanal. Chem. 2011, 399, 2711.
- [15] D. Weibel, S. Wong, N. Lockyer, P. Blenkinsopp, R. Hill, J. C. Vickerman, *Anal. Chem.* 2003, 75, 1754.
- [16] Y. Yamamoto, K. Ichiki, S. Ninomiya, T. Seki, T. Aoki, J. Matsuo, in Ion Implantation Technology 2010 (Eds: J. Matsuo, M. Kase, T. Aoki, T. Seki), AIP, New York, **2010**, pp. 298–301.
- [17] T. Aoki, J. Matsuo, G. Takaoka, Nucl. Instrum. Methods Phys. Res. B 2003, 202, 278.

[18] J. L. S. Lee, S. Ninomiya, J. Matsuo, I. S. Gilmore, M. P. Seah, A. G. Shard, *Anal. Chem.* **2010**, *82*, 98.

J. Lovrić et al.

- [19] D. M. Omiatek, M. F. Santillo, M. L. Heien, A. G. Ewing, Anal. Chem. 2009, 81, 2294.
- [20] A. Gunnarsson, F. Kollmer, S. Sohn, F. Höök, P. Sjövall, Anal. Chem. 2010, 82, 2426.
- [21] M. S. Long, C. D. Jones, M. R. Helfrich, L. K. Mangeney-Slavin, C. D. Keating, Proc. Natl. Acad. Sci. U. S. A. 2005, 102, 5920.
- [22] I. Lanekoff, M. E. Kurczy, R. Hill, J. S. Fletcher, J. C. Vickerman, N. Winograd, P. Sjövall, A. G. Ewing, Anal. Chem. 2010, 82, 6652.
- [23] R. N. S. Sodhi, Analyst (Cambridge, U. K.) 2004, 129, 483.
- [24] J. S. Fletcher, S. Rabbani, A. Henderson, N. P. Lockyer, J. C. Vickerman, *Rapid Commun. Mass Spectrom.* 2011, 25, 925.
- [25] A. G. Shard, F. M. Green, P. J. Brewer, M. P. Seah, I. S. Gilmore, J. Phys. Chem. B 2008, 112, 2596.
- [26] H. Hotani, F. Nomura, Y. Suzuki, Curr. Opin. Colloid Interface Sci. 1999, 4, 358.
- [27] A. Nasedkin, J. Davidsson, M. Kumpugdee-Vollrath, J. Synchrotron Radiat. 2013, 20, 721.

Supporting information

Additional supporting information may be found in the online version of this article at the publisher's web-site.