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Dopamine Release Dynamics in the Tuberoinfundibular Dopamine System

Stefanos Stagkourakis,¹ Johan Dunevall,² Zahra Taleat,³ Andrew G. Ewing,³ and Christian Broberger¹

¹Department of Neuroscience, Karolinska Institutet, 17165 Stockholm, Sweden, ²Department of Chemistry and Chemical Engineering, Chalmers University of Technology, 41296 Gothenburg, Sweden, and ³Department of Chemistry and Molecular Biology, University of Gothenburg, 41296 Gothenburg, Sweden

The relationship between neuronal impulse activity and neurotransmitter release remains elusive. This issue is especially poorly understood in the neuroendocrine system, with its particular demands on periodically voluminous release of neurohormones at the interface of axon terminals and vasculature. A shortage of techniques with sufficient temporal resolution has hindered real-time monitoring of the secretion of the peptides that dominate among the neurohormones. The lactotropic axis provides an important exception in neurochemical identity, however, as pituitary prolactin secretion is primarily under monoaminergic control, via tuberoinfundibular dopamine (TIDA) neurons projecting to the median eminence (ME). Here, we combined electrical or optogenetic stimulation and fast-scan cyclic voltammetry to address dopamine release dynamics in the male mouse TIDA system. Imposing different discharge frequencies during brief (3 s) stimulation of TIDA terminals in the ME revealed that dopamine output is maximal at 10 Hz, which was found to parallel the TIDA neuron action potential frequency distribution during phasic discharge. Over more sustained stimulation periods (150 s), maximal output occurred at 5 Hz, similar to the average action potential firing frequency of tonically active TIDA neurons. Application of the dopamine transporter blocker, methylphenidate, significantly increased dopamine levels in the ME, supporting a functional role of the transporter at the neurons' terminals. Lastly, TIDA neuron stimulation at the cell body yielded perisomatic release of dopamine, which may contribute to an ultrafast negative feedback mechanism to constrain TIDA electrical activity. Together, these data shed light on how spiking patterns in the neuroendocrine system translate to vesicular release toward the pituitary and identify how dopamine dynamics are controlled in the TIDA system at different cellular compartments.

Key words: arcuate nucleus; dopamine release; frequency coding; FSCV; hypothalamus; tuberoinfundibular

Significance Statement

A central question in neuroscience is the complex relationship between neuronal discharge activity and transmitter release. By combining optogenetic stimulation and voltammetry, we address this issue in dopamine neurons of the neuroendocrine system, which faces particular spatiotemporal demands on exocytotic release; large amounts of neurohormone need to be secreted into the portal capillaries with precise timing to adapt to physiological requirements. Our data show that release is maximal around the neurons' default firing frequency. We further provide support for functional dopamine transport at the neurovascular terminals, shedding light on a long-standing controversy about the existence of neuroendocrine transmitter reuptake. Finally, we show that dopamine release occurs also at the somatodendritic level, providing a substrate for an ultrashort autoregulatory feedback loop.

Introduction

The relationship between neuronal impulse traffic and the amount of transmitter released at the axonal terminal has en-

gaged neuroscience since the initial description of quantal release (Del Castillo and Katz, 1954). A question triggered by these seminal observations on the effects of a single action potential was how different patterns and frequencies of discharge translate into

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S. Stagkourakis's present address: Department of Biology and Biological Engineering, Caltech, 91125 Pasadena, USA.

Correspondence should be addressed to Stefanos Stagkourakis at stefanos.stagkourakis@caltech.edu or Christian Broberger at christian.broberger@ki.se.

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neurotransmitter exocytosis. The conversion from electrical (action potential) to chemical (Ca^{2+} -dependent vesicle release and subsequent receptor binding) identity of the neuronal signal introduces several nonlinearities into the process, which complicate the relationship between discharge pattern and secretion. This issue has been addressed in the well-characterized dopaminergic substantia nigra and ventral tegmental area populations, projecting to the caudate-putamen and nucleus accumbens, respectively, revealing the frequency dependence of dopamine output (L. Zhang et al., 2009; Bass et al., 2010). Thus, mesencephalic dopamine terminals exhibit a preferred frequency for optimal neurotransmitter output. Such a mechanism allows neurons to recruit different vesicle and neurotransmitter pools (Iverfeldt et al., 1989; Liu et al., 2011; Doussau et al., 2017), increasing the computational capacity of individual cells. It also provides a safety mechanism, as low activity often will not translate to substantial output (Ngodup et al., 2015).

The neuroendocrine system exhibits several features that distinguishes it from canonical CNS circuits. Instead of a postsynaptic neuron, the targets of the parvocellular systems consist of the endocrine cells of the anterior pituitary gland, which the releasing and inhibiting factors of the neuroendocrine neurons reach by way of the portal capillaries following release at the neurovascular interface (Harris, 1948a,b). The demands on neurohormone volume that follow from this structural organization likely differ substantially from those required to elicit action within the prototypical synapse. Furthermore, the secretion of signal substances into the bloodstream rather than into a confined synaptic cleft suggests that conditions for signal substance reuptake, if it occurs at all, may be different. However, these issues have been difficult to explore because of the lack of high-resolution techniques in the temporal domain to quantitatively measure release of neuropeptides and/or neurohormones (with rare exceptions; Glanowska et al., 2012).

Among the hypothalamo-pituitary systems, the lactotropic axis stands out, however, because of its inhibitory effect on target cells and the monoaminergic nature of its chemical signal. Tuberoinfundibular dopamine (TIDA) neurons located in the dorsomedial arcuate nucleus (dmArc) provide a powerful suppressive influence on pituitary lactotrope cells, which produce the hormone, prolactin (Lyons and Broberger, 2014; Grattan, 2015). Prolactin, in turn, plays an important role in, for example, reproduction. A surge in circulating prolactin during late pregnancy and lactation triggers several important physiological functions in the mother, including lactation and maternal care (Grattan, 2015). Dopamine, released in the median eminence (ME) for passage to the hypophyseal portal blood circulation, tonically inhibits the lactotropes through dopamine D2-type receptors (Gudelsky, 1981; Malgaroli et al., 1987; Israel et al., 1990; Lledo et al., 1990; Stefanescu et al., 2000). Recent studies have revealed distinguishing electrophysiological characteristics of TIDA cells (Lyons et al., 2010), including the capacity for a variable repertoire of firing frequencies in mouse neurons (Romanò et al., 2013; Stagkourakis et al., 2018).

Dopamine release can be monitored with high temporal precision and chemical specificity through fast-scan cyclic voltammetry (FSCV) (Baur et al., 1988; Robinson et al., 2003; Rodeberg et al., 2017). Here, we used electrical (Garris et al., 1997) and optogenetic stimulation (Brimblecombe et al., 2015; Melchior et al., 2015) to impose different discharge protocols upon mouse TIDA neurons and recorded the resultant dopamine release at different cellular compartments. The results provide evidence for frequency optimization, functional reuptake through the dopa-

mine transporter (DAT) at TIDA terminals, and a recently proposed ultrashort autoinhibitory feedback loop (Stagkourakis et al., 2016).

Materials and Methods

Animals. All animal experiments had received approval from the local ethical board, Stockholms Norra Djurförsöksetiska Nämnd, and were performed in accordance with the European Communities Council Directive of November 24, 1986 (86/609/EEC). WT mice with C57BL/6J and BALB/c background were used, in addition to previously generated C57BL/6J *Slc6a*^{Cre} (DAT-Cre) knock-in (Ekstrand et al., 2007) and floxed-tdTomato mice (The Jackson Laboratory, strain datasheet 007909). Animals were group-housed, up to 5 per cage, in a temperature-controlled (23°C) and humidity-controlled (55%) environment, in a 12/12 h light/dark cycle with *ad libitum* access to food and water. Cages were changed on a weekly basis.

Viral vectors. For channelrhodopsin *in vitro* optogenetic studies animals were microinjected (see below) in the dmArc with 250 nl of AAV5-EF1a-DIO-hChr2(H134R)-eYFP-WPRE-hGH (Addgene, 20298) 8.41×10^{12} genomic copies per milliliter. Control groups were injected with 250 nl of AAV5-EF1a-DIO-eYFP-WPRE-hGH (Addgene, 27056) 5.82×10^{12} genomic copies per milliliter. The Chr2 and control eYFP AAV5s were prepared by the University of Pennsylvania Vector Core.

Stereotaxic surgery and viral gene transfer. Adult DAT-Cre male mice of 3–6 months age (sexually inexperienced) were stereotactically injected with a virus (see below) and subsequently individually housed for 2 weeks after surgery. Animals were anesthetized with isoflurane (1%–5%) and placed in a stereotaxic frame (David Kopf Instruments). Virus was bilaterally injected into the dmArc using a pulled glass capillary (World Precision Instruments) by nanoliter pressure injection at a flow rate of 50 nl per minute (Micro4 controller, World Precision Instruments; Nanoinjector II, Drummond Scientific). Stereotaxic injection coordinates (bregma: -1.8 mm, midline ± 0.1 mm, dorsal surface -5.5 mm) to target the dmArc were obtained from the Paxinos and Franklin atlas (Franklin and Paxinos, 2008). The rostrocaudal extent of viral infections was confined to the dmArc, and transduced DAT positive neurons were typically found between -1.5 mm and -2.00 mm from bregma, yielding two useful brain slices per animal.

Brain slice electrophysiology. Acute slices of the mediobasal hypothalamus were prepared from adult DAT-tdTomato mice. Slices were cut on a vibratome (Leica Microsystems VT1000S) to 250 μm thickness and continuously perfused with oxygenated aCSF containing the following (in mM): 127 NaCl, 2.0 KCl, 1.2 NaH_2PO_4 , 26 NaHCO_3 , 1.3 MgCl_2 , 2.4 CaCl_2 , and 10 D-glucose, at $32 \pm 1^\circ\text{C}$ during recording. Each slice was exposed only to a single bath application of pharmacological compounds and was used for a single experiment. Whole-cell current- and voltage-clamp recordings were performed with micropipettes filled with intracellular solution containing the following (in mM), 140 K-gluconate, 10 KCl, 10 HEPES, 10 EGTA, and 2 Na_2ATP , pH 7.3, with KOH. Recordings were performed using a Multiclamp 700B amplifier, a DigiData 1440 digitizer, and pClamp 10.2 software (Molecular Devices). Slow and fast capacitative components were semiautomatically compensated. Access resistance was monitored throughout the experiments, and neurons in which the series resistance exceeded 15 $\text{M}\Omega$ or changed $\geq 20\%$ were excluded from further analysis. Liquid junction potential was 16.4 mV and not compensated. The recorded current was sampled at 20 kHz.

For *in vitro* optogenetics during slice whole-cell recordings, photostimulation was generated through a 3.4 W 447 nm LED mounted on the microscope oculars and delivered through the objective lens. Photostimulation was controlled via the analog outputs of a DigiData 1440A, enabling control over the duration and intensity. The photostimulation diameter through the objective lens was ~ 350 μm with illumination intensity typically scaled to 3 mW/mm^2 . MATLAB (The MathWorks) and OriginPro 8 (OriginLab) were used for electrophysiological data analysis.

Immunofluorescence. Mice were anesthetized with sodium pentobarbital (200 mg/kg, i.p., Sanofi-Aventis), then transcardially perfused with 10 ml Ca^{2+} -free Tyrode's solution (37°C) containing 0.2% heparin, fol-

lowed by 10 ml fixative (4% PFA and 0.4% picric acid in 0.16 M PBS, 37°C), and then 50 ml ice-cold fixative. Whole brains were dissected, immersed in ice-cold fixative for 90 min, and then stored in 0.1 M PBS, pH 7.4, containing 20% sucrose, 0.02% bacitracin, and 0.01% sodium azide for 3 d, before freezing with CO₂. Coronal sections were cut at a thickness of 14 μm using a cryostat (Microm) and thaw-mounted onto gelatin-coated glass slides. For indirect immunofluorescence staining (performed at room temperature unless otherwise specified), air-dried sections were washed in 0.01 M PBS for 30 min before incubation with the primary antibody diluted in PBS containing 0.3% Triton X-100 and 1% BSA for 16 h at 4°C. The slides were then washed for 30 min in PBS followed by 2 h incubation with Alexa-488-conjugated donkey anti-rabbit secondary antisera (1:500; Invitrogen). Immunohistochemistry for pSTAT5: Before immunofluorescence staining, antigen retrieval was performed by incubating sections for 15 min in citric acid, pH 7.4, at 80°C, and then cooled at room temperature for a further 30 min. After a 1% H₂O₂ Tris-buffered wash, sections were incubated in rabbit pSTAT5 primary antibody (pSTAT5 Tyr 694, catalog #C11C5, 1:500; Cell Signaling Technology) for 72 h at 4°C. Primary antibody incubation was followed by Cy5-conjugated donkey anti-rabbit secondary antisera (1:500; Invitrogen). TH immunoreactivity was detected via anti-TH antiserum (1:2000; raised in rabbit, AB152, Millipore), and was followed by Alexa488-conjugated goat raised anti-rabbit secondary antisera (1:500; Invitrogen). Slides were incubated with the nuclear marker DAPI (Invitrogen) diluted 1:10,000 in PBS for 5 min before a final wash for 30 min in PBS, and mounted with glycerol containing (2.5% DABCO; Sigma-Aldrich).

TIDA cell identification in C57 WT mice. TIDA neuron recordings from C57 WT mice were performed in dmArc using intracellular solution containing 0.2% Neurobiotin. After recording, slices were placed in fixative (4% PFA/0.16% picric acid), washed in PBS, and incubated at 4°C for 72 h in a solution containing FITC-conjugated avidin (1:2500, 43-4411, Zymed) and rabbit anti-TH immunoglobulin (1:2000, AB152, Millipore). Following washing, slices were incubated in secondary Alexa-594-conjugated donkey-anti-rabbit antiserum (1:500; Invitrogen; A21202) for 24 h at 4°C, washed again, and mounted with 2.5% DABCO in glycerol. Cells colocalizing FITC and TH in the dmArc were considered as TIDA neurons.

ISH. DAT-Cre-floxed-tdTomato mice were anesthetized with pentobarbital, killed by decapitation, and the brains were rapidly removed and frozen on dry ice; 10-μm-thick coronal sections were cut using a cryostat and thaw-mounted onto SuperFrost glass slides. Sections were fixed in 4% PFA for 15 min at 4°C and then dehydrated through incubation in 50% EtOH (1 × 5 min), 70% EtOH (1 × 5 min), and last 100% EtOH (2 × 5 min). Slides were air-dried for 10 min, and a hydrophobic barrier was created around each section using the ImmEdge pen (Vector Laboratories). ISH was performed using a modification of the RNAscope (Advanced Cell Diagnostics) protocol. Pretreat 4 (ACDBio, RNAscope Fluorescent Multiplex Reagent Kit, 320850) was added to entirely cover the sections for 30 min at room temperature. After PBS washing, sections were incubated with Mm-Th-C3 (317621-C3), Mm-Slc6a3-C2 (315441-C2), and tdTomato (317041) RNAscope probes for 2 h at 40°C using the HybEZ Humidifying System (ACDBio). The following incubation steps were then performed: Amp 1-FL for 30 min at 40°C, Amp 2-FL for 15 min at 40°C, Amp 3-FL for 30 min at 40°C, and Amp 4-FL-AltB for 15 min at 40°C (320850). Wash buffer (320850) was used to rinse the slides after each step. Sections were incubated with DAPI solution (320850) for 30 s at room temperature, and ProLong Gold Antifade Mountant (Thermo Fisher Scientific) was added before placing the coverslips. Quantification of mRNA coexistence within cells was performed on confocal Z-stack dmArc images acquired at 40× magnification.

Confocal microscopy. Brain slices were imaged by epifluorescence microscopy (Carl Zeiss, Imager M1) or confocal microscopy (Carl Zeiss, LSM 800) for subsequent analysis. Brain areas were determined according to their anatomy using Paxinos and Franklin brain atlas (Franklin and Paxinos, 2008).

Carbon fiber microelectrodes. Carbon fiber electrodes were fabricated by aspirating 7-μm-diameter carbon fibers (Cytec Engineered Materials) into borosilicate glass capillaries (1.2 mm O.D., 0.69 mm I.D., Sutter

Instrument). The capillaries were subsequently pulled with a commercial micropipette puller (Sutter Instrument, P-97) and sealed with epoxy (EpoTek 301, Epoxy Technology). The electrode tips were polished at a 45° angle on a diamond dust-embedded micropipette-beveling wheel (model BV-10, Sutter Instrument). Electrodes were tested in solutions of known concentrations of dopamine. Only electrodes showing reaction kinetics typical of dopamine (as examined in current vs time plots, and current vs voltage plots) were used.

FSCV. A Chem-Clamp potentiostat (Dagan) and two data acquisition boards (PCI-6221, National Instruments) run by the TH 1.0 CV program (ESA) were used to collect all electrochemical data. Cyclic voltammograms were obtained by applying a triangular waveform potential (−0.4 to 1.3 V vs Ag/AgCl) repeated every 100 ms at a scan rate of 200 V/s (low pass Bessel filter at 3 kHz). Each cyclic voltammogram was a background-subtracted average of 10 successive cyclic voltammograms taken at the maximum oxidation peak current. All electrodes were allowed to cycle for at least 15 min before recording to stabilize the background current. The recorded current response was converted to dopamine concentration via *in vitro* electrode calibration in a standard dopamine solution after each experiment. Acquired data were analyzed and plotted using MATLAB routines, and statistical analysis was performed using Prism 6.0 (GraphPad). Last, bath application of the DAT blocker methylphenidate in isolation (i.e., in the absence of a brain slice) did not generate oxidative current during FSCV recordings ($n = 3$). Methylphenidate hydrochloride (M2892, Sigma-Aldrich) was dissolved in aCSF and was bath applied via gravitational flow. TTX was purchased from Alomone Labs (CAS #18660–81–6) and dissolved in deionized H₂O. 4-AP (275875) and cadmium chloride (CdCl₂, 275875) were purchased from Sigma-Aldrich, and were dissolved in deionized H₂O.

Extracellular stimulation. Electrical stimulation of the external zone of the lateral ME was performed with borosilicate glass microcapillaries (same as used for patch recordings), connected to a stimulus isolation unit (MI401; Zoological Institute, University of Cologne, Cologne, Germany). The stimulation intensity was set to 2× the minimal stimulus intensity required to reliably evoke dopamine release events using a stimulation protocol of 3 s, 10 Hz, and 5 ms pulse width and typically scaled between 10 and 100 mA in amplitude. Only WT C57BL/6J mice were used on FSCV recordings with electrically evoked dopamine release.

Experimental design and statistical analysis. Immunohistochemistry and *in situ* data were collected from a minimum of 8 animals, each animal contributing a single or two sections per dataset. Electrophysiology data were collected from 10 animals, each animal contributing four or five cells in the dataset. FSCV data were collected from multiple brain slices collected from a minimum of 3 individual animals on consequent experimental days. A minimum of five recordings represent each FSCV data group. All *t* tests and one-way ANOVAs were performed using Prism software (GraphPad). The appropriate *post hoc* test was used for each one-way ANOVA. Normality was determined by D'Agostino-Pearson normality test. Statistical significance was set at $p < 0.05$.

Results

Absence of detectable spontaneous dopamine release in coronal hypothalamic slices

TIDA neurons (Fig. 1A) were targeted for recording using DAT-tdTomato mice (Fig. 1B–D). To evaluate the coexpression between TH and DAT, and the DAT-Cre mouse line as an appropriate model for identifying TIDA cells, we performed triple-label ISH for TH, DAT, and tdTomato in hypothalamic brain sections from DAT-tdTomato mice (Fig. 1E). The majority (84%) of cells expressed all three mRNA species, suggesting that the DAT-Cre line offers a suitable model for investigation of TIDA neuron physiology (i.e., dopaminergic neurons in the dmArc; Fig. 1F).

Whole-cell patch-clamp recordings confirmed that mouse TIDA neurons exhibit a diverse range of firing rates *in vitro* in agreement with earlier reports (Romanò et al., 2013; X. Zhang and van den Pol,

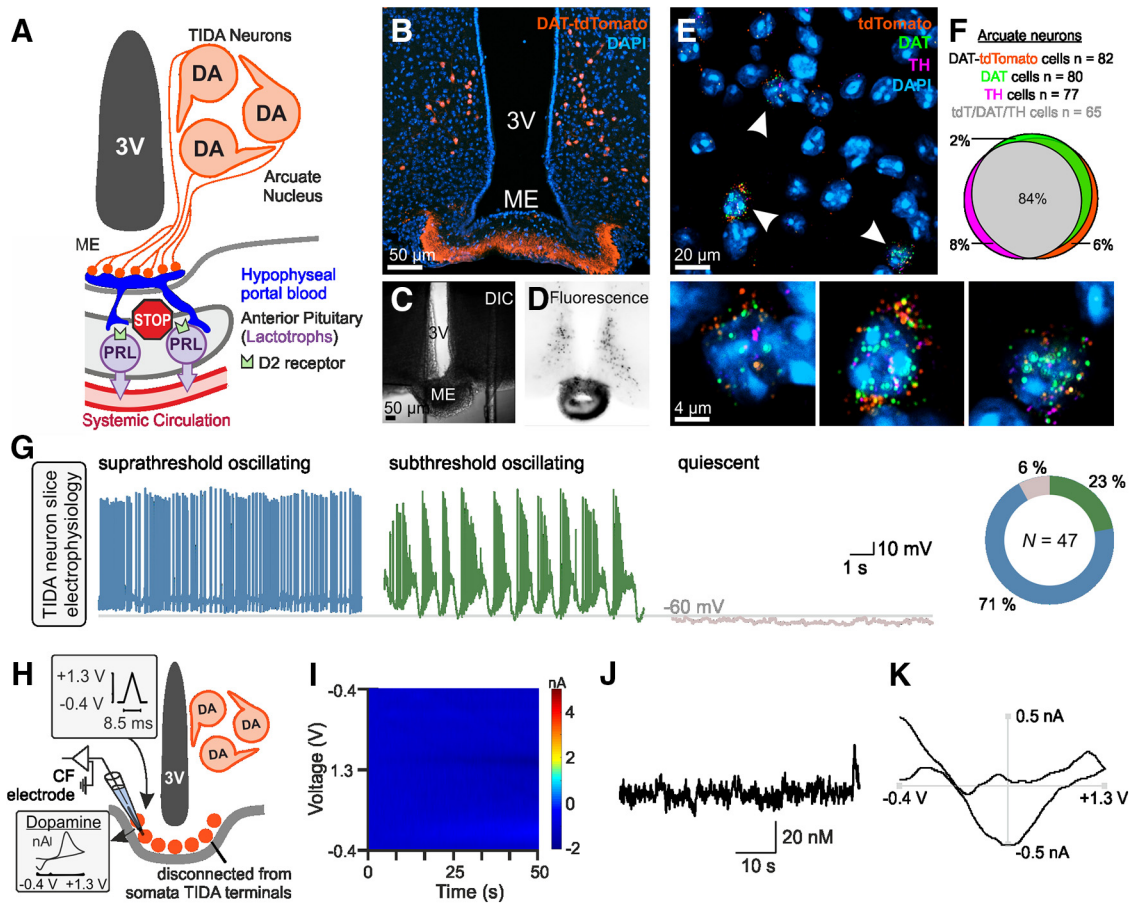


Figure 1. TIDA neuron preparation and absence of detectable spontaneous dopamine release in the ME in acute hypothalamic slices. **A**, Schematic illustration of the lactotropic axis and the TIDA neuron projection to the ME. **B–D**, DAT promoter-driven expression of tdTomato for the identification of TIDA cells after fixation (**B**) and in acute brain slices used for electrophysiology visualized in differential interference contrast (DIC) (**C**), and in fluorescence (**D**, converted to black and white and inverted) illumination, respectively. **E**, ISH for the TH, DAT, and tdTomato mRNA to quantify TH-, DAT-, and Cre-mediated expression of floxed constructs in the DAT-Cre mouse line (top). High magnification of three cells indicated via white arrows in **E** (bottom). **F**, Quantification of TH, DAT, and tdTomato mRNA coexistence in cell bodies reveals an 84% colocalization between the three transcripts ($N = 16$ confocal images collected from $N = 8$ arcuate containing sections [-1.8 mm from bregma] from 8 mice). **G**, Mouse TIDA neurons exhibit various patterns of activity, suprathreshold oscillations (left), subthreshold oscillations (middle), and quiescent behavior (right). Quantification of the proportion of TIDA neurons exhibiting the different forms of activity presented in the far right. **H**, Schematic drawing illustrating the use of FSCV and carbon fiber (CF) disc electrodes to measure TIDA neural activity with neurotransmitter (dopamine) release in the ME. **I–K**, Representative color plot (**I**), current versus time plot (**J**), and voltammogram (**K**) generated through voltammetric measurements revealing no spontaneous dopamine release above detection threshold (5–10 nM) in the ME ($N = 20$ recordings from $N = 10$ slices from $N = 5$ mice). 3V, Third ventricle.

2015; Stagkourakis et al., 2018) (Figure 1G). The majority (71%) of TIDA cells were found to have a tonic firing pattern with phasic alterations in firing frequency, echoed in phasic fluctuations in membrane voltage (Fig. 1G, middle). Approximately one-fourth of the cells exhibited oscillatory, rhythmic firing interspersed with brief (~500 ms) periods of quiescence (Fig. 1G, left). A small fraction of the TIDA neurons in the slice preparation were consistently hyperpolarized and quiescent (Fig. 1G, right).

As TIDA neurons are spontaneously active *in vitro*, we first asked whether baseline dopamine release can be detected at the site of the terminals in the slice preparation. Carbon fiber electrodes were thus placed in the ME, and an adapted FSCV protocol from Kosillo et al. (2016) was applied (Fig. 1H). In this configuration, no dopamine signal could be observed above the detection threshold (~10 nM; $N = 20$ recordings from $N = 10$ slices from $N = 5$ mice; Fig. 1I–K). One possible reason for this failure to detect dopamine may be that the axons connecting the TIDA cell somata in the dmArc and the terminals in the ME are largely severed in the coronal slice preparation, as indicated by cytoarchitectonic studies (van den Pol and Cassidy, 1982), interrupting impulse traffic. Similar observations have occurred in other dopamine systems, such as in the striatum (Threlfell et al., 2012;

O'Neill et al., 2017) and nucleus accumbens (Melchior and Jones, 2017), where the absence of spontaneous dopamine release in slice preparations has motivated electrically or optically evoked investigations of dopamine release dynamics at different conditions. We therefore next sought to identify evoked dopamine release properties via optogenetic stimulation of the TIDA terminals. This strategy offers the benefit that the dynamics of the transmitter release at the level of the terminals, on the one hand, and at the somatodendritic level on the other, can be studied separately.

Stable electrically and optically evoked dopamine release in the ME

To enable dopamine release from the terminals, we first used extracellular electrical stimulation of the lateral part of the ME during voltammetric recordings using brain slices from C57 WT mice (Fig. 2A). Electrical stimulation of the ME led to reliable, stable dopamine release over time when tested with 5 min sampling interval (Fig. 2B, E; $N = 5$, $F_{(2,258,9,034)} = 0.3811$, $df = 6$, $p = 0.7171$, repeated-measures one-way ANOVA; Table 1). Next, to study optogenetically evoked dopamine release, DAT-Cre animals were bilaterally injected in the dmArc with AAV-DIO-ChR2-eYFP-hGH. One month later, FSCV recordings were

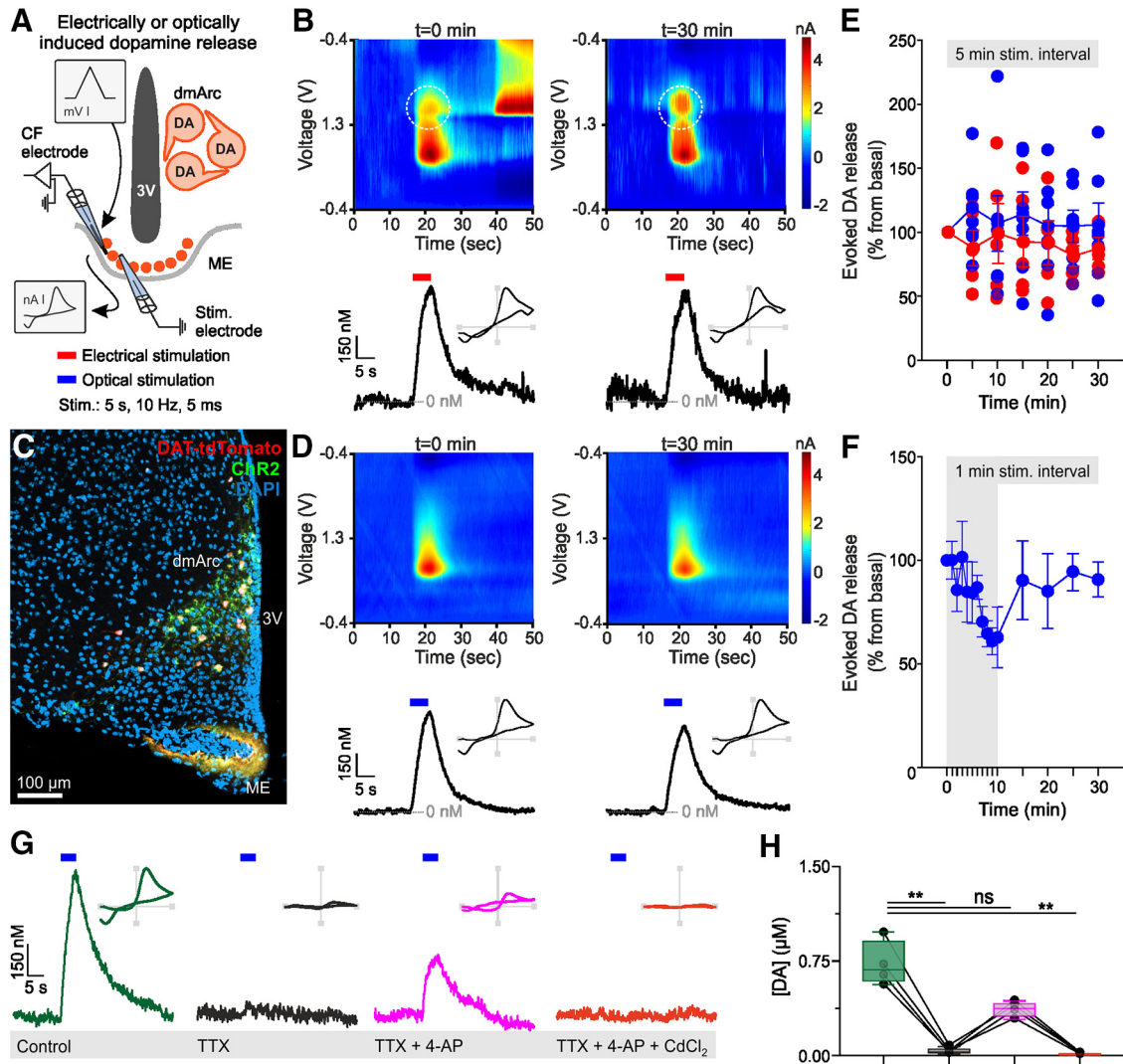


Figure 2. Evoked dopamine release in the ME is stable over time. **A**, Schematic drawing illustrating the use of FSCV with electrically and optically evoked dopamine release in the ME. **B**, Electrically evoked dopamine release at $t = 0$ min and 30 min after, in arcuate slices from WT C57BL/6J mice (dashed circle line/peak represents the electrical stimulation artifact or another oxidizing substance released in the ME following the stimulus). **C**, Confocal Z-stack micrograph illustrating virally mediated Chr2-eYFP expression in the dmArc in the DAT-tdTomato mouse. The Chr2-eYFP and DAT-tdTomato fluorescence in the ME. **D**, Optogenetically evoked dopamine release at $t = 0$ min and 30 min later, in arcuate slices from DAT-Cre mice of C57BL/6J background. **E**, Both electrically (red) and optically evoked (blue) dopamine release with a 5 min stimulation interval is sustainable over time ($N = 5-7$ per group, repeated-measures one-way ANOVA, $p > 0.05$; Table 1). **F**, Evoked dopamine release with a 1 min stimulation interval leads to a reversible dopamine depletion, reversible upon return to a 5 min stimulation interval ($N = 5$ per group, repeated-measures one-way ANOVA, $p < 0.0001$). **G**, Representative FSCV traces with Chr2-evoked dopamine release in control conditions: versus in the presence of the Na⁺ channel blocker TTX, versus coapplication of TTX and the K⁺ channel blocker 4-AP, and versus coapplication of TTX + 4-AP and the nonselective Ca²⁺ channel blocker CdCl₂. **H**, Quantification of dopamine release in different conditions illustrated in **G** (repeated-measures one-way ANOVA, $p = 0.0032$; Table 1). ** $p < 0.01$. Data are mean \pm SEM. 3V, Third ventricle.

performed *in vitro* to test for optically evoked dopamine release (Fig. 2A, C). Using a stimulation protocol of 5 s in duration and 10 Hz frequency stimulation with 5 ms pulse width, robust and stable dopamine release was recorded from the ME (Fig. 2D, E) similarly to what was observed with electrically evoked dopamine measurements. To test for the possibility of dopamine depletion at the terminals with repeated stimulation, we performed recurrent photostimulation at different time intervals (1 or 5 min). Photostimulation with 5 min interval resulted in stable evoked release at near 100% of the initial levels, throughout a 30 min period (Fig. 2E; $N = 7$, $F_{(3,161,18,96)} = 0.2747$, $df = 6$, $p = 0.8522$, repeated-measures one-way ANOVA; Table 1), whereas photostimulation with 1 min intervals resulted in attenuation of the dopamine signal to near 50% of the basal levels over 10 min (Fig. 2F; $N = 5$, $F_{(3,036,12,14)} = 2.188$, $df = 14$, $p = 0.1413$, repeated-measures one-way ANOVA; Table 1). Once the longer (5 min)

photostimulation interval was reinstated, however, the dopamine signal recovered to initial levels (Fig. 2F). Previous work has suggested that AAVs containing the hGH minigene can potentially alter excitability of transduced endocrine cells (Brouwers et al., 2014). Because the viral constructs used in the present study contain the hGH minigene, control experiments were performed to address whether this construct might influence TIDA behavior. However, quantification of firing rates and pSTAT5 immunoreactivity (as a marker of prolactin receptor activation via hGH) (Goffin and Kelly, 1997; Buteau et al., 1998) in C57 WT, DAT-tdTomato, and DAT-Cre mice injected with AAV-DIO-eYFP-hGH did not yield any changes related to hGH expression (Fig. 3A–D; Table 1).

Importantly, optically evoked dopamine release was found to be sensitive to application of TTX (500 nM), whereas coapplication of TTX (500 nM) and 4-AP (100 μ M) led to partial recovery

Table 1. Statistics

| Figures | Test | N | F or t | df | p | Multiple comparisons | Adjusted p | p summary |
|---|--|-------|------------------------------|----|---------|---|------------|-----------|
| Figure 2E (electrical stimulation; in red) | Repeated-measures one-way ANOVA with Dunnett's multiple comparisons test | 5 | $F_{(2,258,9,034)} = 0.3811$ | 6 | 0.7171 | 0 min versus 5 min | 0.8652 | NS |
| | | | | | | 0 min versus 10 min | >0.9999 | NS |
| | | | | | | 0 min versus 15 min | 0.9961 | NS |
| | | | | | | 0 min versus 20 min | 0.9891 | NS |
| | | | | | | 0 min versus 25 min | 0.2479 | NS |
| | | | | | | 0 min versus 30 min | 0.5699 | NS |
| Figure 2E (optical stimulation; in blue) | Repeated-measures one-way ANOVA with Dunnett's multiple comparisons test | 7 | $F_{(3,161,18,96)} = 0.2747$ | 6 | 0.8522 | 0 min versus 5 min | 0.5051 | NS |
| | | | | | | 0 min versus 10 min | 0.9983 | NS |
| | | | | | | 0 min versus 15 min | 0.8838 | NS |
| | | | | | | 0 min versus 20 min | 0.9983 | NS |
| | | | | | | 0 min versus 25 min | 0.9960 | NS |
| | | | | | | 0 min versus 30 min | 0.9968 | NS |
| Figure 2F | Repeated-measures one-way ANOVA with Dunnett's multiple comparisons test | 5 | $F_{(3,036,12,14)} = 2.188$ | 14 | 0.1413 | 0 min versus 1 min | >0.9999 | NS |
| | | | | | | 0 min versus 2 min | 0.7617 | NS |
| | | | | | | 0 min versus 3 min | 0.9999 | NS |
| | | | | | | 0 min versus 4 min | 0.9156 | NS |
| | | | | | | 0 min versus 5 min | 0.9098 | NS |
| | | | | | | 0 min versus 6 min | 0.3838 | NS |
| | | | | | | 0 min versus 7 min | 0.0835 | NS |
| | | | | | | 0 min versus 8 min | 0.0256 | * |
| | | | | | | 0 min versus 9 min | 0.0218 | * |
| | | | | | | 0 min versus 10 min | 0.2914 | NS |
| | | | | | | 0 min versus 15 min | 0.9977 | NS |
| | | | | | | 0 min versus 20 min | 0.9725 | NS |
| | | | | | | 0 min versus 25 min | 0.9941 | NS |
| | | | | | | 0 min versus 30 min | 0.8931 | NS |
| | | | | | | Control versus TTX | 0.0068 | ** |
| Control versus TTX + 4-AP | 0.0757 | NS | | | | | | |
| Control versus TTX + 4-AP + CdCl ₂ | 0.0092 | ** | | | | | | |
| Figure 2H (10 ms pulse duration) | one-way ANOVA with Dunnett's multiple comparisons test | 4 | $F_{(3,9)} = 1.282$ | 3 | 0.0032 | Control versus TTX | 0.0068 | ** |
| | | | | | | Control versus TTX + 4-AP | 0.0757 | NS |
| | | | | | | Control versus TTX + 4-AP + CdCl ₂ | 0.0092 | ** |
| | | | | | | | | |
| Figure 3B | one-way ANOVA with Dunnett's multiple comparisons test | 8–12 | $F_{(2,25)} = 0.1192$ | 2 | 0.8881 | C57 wt - TH versus DAT-tdTomato | 0.9889 | NS |
| | | | | | | C57 wt - TH versus DAT-eYFP | 0.9050 | NS |
| | | | | | | C57 wt-TH + pSTAT5 versus DAT-tdTomato + pSTAT5 | 0.8697 | NS |
| | | | | | | C57 wt-TH + pSTAT5 versus DAT-eYFP + pSTAT5 | 0.7708 | NS |
| Figure 3D | One-way ANOVA with Dunnett's multiple comparisons test | 10–33 | $F_{(2,52)} = 0.3014$ | 2 | 0.7411 | DAT-tdTomato versus C57 | 0.9312 | NS |
| | | | | | | DAT-tdTomato versus DAT-eYFP | 0.6881 | NS |
| Figure 4D | Two-tailed paired t test | 6 | 4.357 | 5 | 0.0073 | ** | | |
| Figure 4B | Ordinary one-way ANOVA with Tukey's multiple comparisons test | 33 | $F_{(14,338)} = 17.08$ | 14 | <0.0001 | 1st versus 4th AP | <0.0001 | **** |
| | | | | | | 2nd versus 4th AP | <0.0001 | **** |
| | | | | | | 5th versus 10th AP | >0.9999 | NS |
| | | | | | | 10th versus 14th AP | 0.0132 | * |
| | | | | | | 10th versus 15th AP | 0.0117 | * |
| Figure 4F (2 ms pulse duration, optical stimulation) | Repeated-measures one-way ANOVA with Dunnett's multiple comparisons test | 6 | $F_{(1,935,9,677)} = 100.6$ | 6 | <0.0001 | 2 Hz versus 5 Hz | >0.9999 | NS |
| | | | | | | 2 Hz versus 10 Hz | 0.0364 | * |
| | | | | | | 2 Hz versus 20 Hz | <0.0001 | **** |
| | | | | | | 2 Hz versus 30 Hz | 0.0001 | *** |
| | | | | | | 2 Hz versus 40 Hz | <0.0001 | **** |
| | | | | | | 2 Hz versus 50 Hz | <0.0001 | **** |
| Figure 4F (5 ms pulse duration, optical stimulation) | Repeated-measures one-way ANOVA with Dunnett's multiple comparisons test | 5 | $F_{(6,24)} = 100.4$ | 6 | <0.0001 | 2 Hz versus 5 Hz | >0.9999 | NS |
| | | | | | | 2 Hz versus 10 Hz | 0.9932 | NS |
| | | | | | | 2 Hz versus 20 Hz | <0.0001 | **** |
| | | | | | | 2 Hz versus 30 Hz | <0.0001 | **** |
| | | | | | | 2 Hz versus 40 Hz | <0.0001 | **** |
| | | | | | | 2 Hz versus 50 Hz | <0.0001 | **** |
| Figure 4F (10 ms pulse duration, optical stimulation) | Repeated-measures one-way ANOVA with Dunnett's multiple comparisons test | 4 | $F_{(1,503,4,508)} = 72.97$ | 6 | 0.0004 | 2 Hz versus 5 Hz | >0.9999 | NS |
| | | | | | | 2 Hz versus 10 Hz | >0.9999 | NS |
| | | | | | | 2 Hz versus 20 Hz | 0.0595 | NS |
| | | | | | | 2 Hz versus 30 Hz | 0.007 | ** |
| | | | | | | 2 Hz versus 40 Hz | 0.0016 | ** |
| | | | | | | 2 Hz versus 50 Hz | 0.0005 | *** |

(Table continues.)

Table 1. Continued

| Figures | Test | N | F or t | df | p | Multiple comparisons | Adjusted p | p summary |
|---|--|------|----------------------------------|----|---------|----------------------|------------|-----------|
| Figure 4F (5 ms pulse duration, electrical stimulation) | Repeated-measures one-way ANOVA with Dunnett's multiple comparisons test | 9 | $F_{(1,135,10,68)} = 86.62$ | 8 | <0.0001 | 2 Hz versus 5 Hz | >0.9999 | NS |
| | | | | | | 2 Hz versus 10 Hz | >0.9999 | NS |
| | | | | | | 2 Hz versus 20 Hz | <0.0001 | **** |
| | | | | | | 2 Hz versus 30 Hz | <0.0001 | **** |
| | | | | | | 2 Hz versus 40 Hz | <0.0001 | **** |
| | | | | | | 2 Hz versus 50 Hz | <0.0001 | **** |
| Figure 4H (2 ms pulse duration, optical stimulation) | Repeated-measures one-way ANOVA with Dunnett's multiple comparisons test | 6 | $F_{(1,111,8,889)} = 4.124$ | 5 | 0.0706 | 2 Hz versus 5 Hz | 0.268 | NS |
| | | | | | | 2 Hz versus 10 Hz | 0.3002 | NS |
| | | | | | | 2 Hz versus 20 Hz | 0.2444 | NS |
| | | | | | | 2 Hz versus 30 Hz | 0.2637 | NS |
| | | | | | | 2 Hz versus 40 Hz | 0.7629 | NS |
| | | | | | | 2 Hz versus 50 Hz | 0.4558 | NS |
| Figure 4H (5 ms pulse duration, optical stimulation) | Repeated-measures one-way ANOVA with Dunnett's multiple comparisons test | 6 | $F_{(1,067,8,536)} = 5.221$ | 5 | 0.0481 | 2 Hz versus 5 Hz | 0.1586 | NS |
| | | | | | | 2 Hz versus 10 Hz | 0.0442 | * |
| | | | | | | 2 Hz versus 20 Hz | 0.0852 | NS |
| | | | | | | 2 Hz versus 30 Hz | 0.8233 | NS |
| | | | | | | 2 Hz versus 40 Hz | 0.5971 | NS |
| | | | | | | 2 Hz versus 50 Hz | 0.4555 | NS |
| Figure 4H (10 ms pulse duration, optical stimulation) | Repeated-measures one-way ANOVA with Dunnett's multiple comparisons test | 6 | $F_{(6,00,48,00)} = 11.77$ | 5 | <0.0001 | 2 Hz versus 5 Hz | 0.0509 | NS |
| | | | | | | 2 Hz versus 10 Hz | 0.0002 | *** |
| | | | | | | 2 Hz versus 20 Hz | 0.7353 | NS |
| | | | | | | 2 Hz versus 30 Hz | 0.6001 | NS |
| | | | | | | 2 Hz versus 40 Hz | 0.416 | NS |
| | | | | | | 2 Hz versus 50 Hz | 0.2369 | NS |
| Figure 4H (5 ms pulse duration, electrical stimulation, electrical stimulation) | Repeated-measures one-way ANOVA with Dunnett's multiple comparisons test | 5 | $F_{(1,816,7,265)} = 18.98$ | 4 | 0.0015 | 2 Hz versus 5 Hz | 0.0907 | NS |
| | | | | | | 2 Hz versus 10 Hz | 0.0108 | * |
| | | | | | | 2 Hz versus 20 Hz | 0.0710 | NS |
| | | | | | | 2 Hz versus 30 Hz | 0.4024 | NS |
| | | | | | | 2 Hz versus 40 Hz | 0.8639 | NS |
| | | | | | | 2 Hz versus 50 Hz | 0.9965 | NS |
| Figure 5D | Ordinary one-way ANOVA with Tukey's multiple comparisons test | 5 | $F_{(6, 28)} = 5.92$ | 6 | 0.0004 | 0.5 Hz versus 1 Hz | 0.9922 | NS |
| | | | | | | 0.5 Hz versus 2 Hz | 0.4408 | NS |
| | | | | | | 0.5 Hz versus 5 Hz | 0.0016 | ** |
| | | | | | | 0.5 Hz versus 10 Hz | 0.9448 | NS |
| | | | | | | 0.5 Hz versus 20 Hz | >0.9999 | NS |
| | | | | | | 0.5 Hz versus 30 Hz | 0.9973 | NS |
| | | | | | | 1 Hz versus 2 Hz | 0.844 | NS |
| | | | | | | 1 Hz versus 5 Hz | 0.0097 | ** |
| | | | | | | 1 Hz versus 10 Hz | 0.9999 | NS |
| | | | | | | 1 Hz versus 20 Hz | 0.9979 | NS |
| | | | | | | 1 Hz versus 30 Hz | 0.8659 | NS |
| | | | | | | 2 Hz versus 5 Hz | 0.1787 | NS |
| | | | | | | 2 Hz versus 10 Hz | 0.9559 | NS |
| | | | | | | 2 Hz versus 20 Hz | 0.5291 | NS |
| | | | | | | 2 Hz versus 30 Hz | 0.177 | NS |
| | | | | | | 5 Hz versus 10 Hz | 0.0219 | * |
| 5 Hz versus 20 Hz | 0.0024 | ** | | | | | | |
| 5 Hz versus 30 Hz | 0.0004 | *** | | | | | | |
| 10 Hz versus 20 Hz | 0.9734 | NS | | | | | | |
| 10 Hz versus 30 Hz | 0.6909 | NS | | | | | | |
| 20 Hz versus 30 Hz | 0.9907 | NS | | | | | | |
| Figure 5E | One-way Kruskal–Wallis ANOVA | 7 | Kruskal–Wallis statistic — 22964 | p | <0.0001 | Multiple comparisons | Adjusted p | p-summary |
| | | | | | | 0.5 Hz versus 1 Hz | <0.0001 | **** |
| | | | | | | 0.5 Hz versus 2 Hz | <0.0001 | **** |
| | | | | | | 0.5 Hz versus 5 Hz | <0.0001 | **** |
| | | | | | | 0.5 Hz versus 10 Hz | <0.0001 | **** |
| | | | | | | 0.5 Hz versus 20 Hz | <0.0001 | **** |
| | | | | | | 0.5 Hz versus 30 Hz | <0.0001 | **** |
| | | | | | | 1 Hz versus 2 Hz | >0.9999 | NS |
| | | | | | | 1 Hz versus 5 Hz | <0.0001 | **** |
| | | | | | | 1 Hz versus 10 Hz | <0.0001 | **** |
| | | | | | | 1 Hz versus 20 Hz | <0.0001 | **** |
| 1 Hz versus 30 Hz | <0.0001 | **** | | | | | | |

(Table continues.)

Table 1. Continued

| Figures | Test | <i>N</i> | <i>F</i> or <i>t</i> | <i>df</i> | <i>p</i> | Multiple comparisons | Adjusted <i>p</i> | <i>p</i> summary |
|-----------|---------------------------------|--------------|----------------------|-----------|----------|----------------------|-------------------|------------------|
| | | | | | | 2Hzversus 5Hz | <0.0001 | **** |
| | | | | | | 2Hzversus10Hz | <0.0001 | **** |
| | | | | | | 2Hzversus20Hz | <0.0001 | **** |
| | | | | | | 2Hzversus30Hz | <0.0001 | **** |
| | | | | | | 5Hzversus10Hz | <0.0001 | **** |
| | | | | | | 5Hzversus20Hz | <0.0001 | **** |
| | | | | | | 5Hzversus30Hz | <0.0001 | **** |
| | | | | | | 10Hzversus20Hz | <0.0001 | **** |
| | | | | | | 10Hzversus30Hz | <0.0001 | **** |
| | | | | | | 20Hzversus30Hz | <0.0001 | **** |
| | | No. of pairs | <i>t</i> | <i>df</i> | | | | |
| Figure 6B | Two-tailed paired <i>t</i> test | 6 | 4.439 | 5 | 0.0068 | | | ** |
| Figure 6C | Two-tailed paired <i>t</i> test | 6 | 0.4974 | 5 | 0.6400 | | | NS |
| Figure 6D | Two-tailed paired <i>t</i> test | 6 | 5.228 | 5 | 0.0034 | | | ** |
| Figure 6E | Two-tailed paired <i>t</i> test | 6 | 1.115 | 5 | 0.3154 | | | NS |

p* < 0.05; *p* < 0.01; ****p* < 0.001; *****p* < 0.0001.

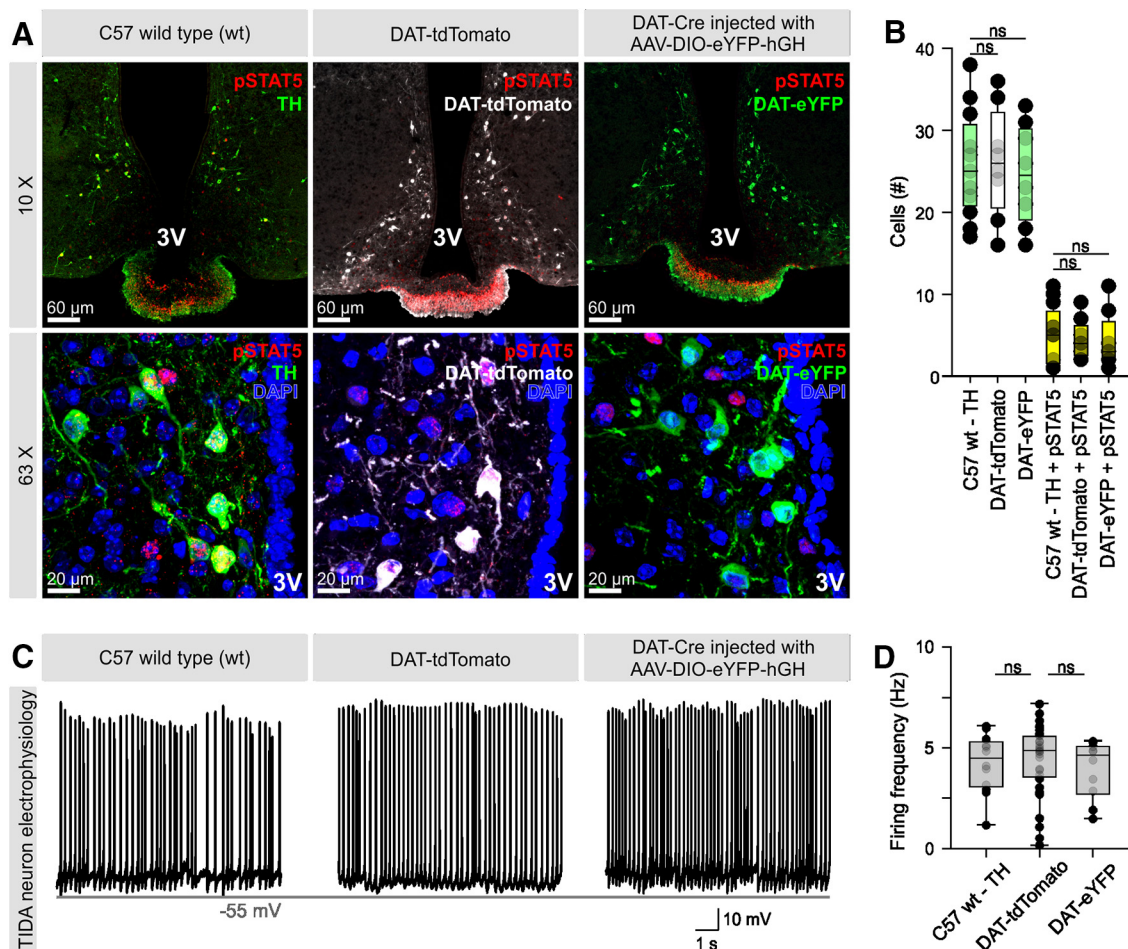


Figure 3. Expression of the hGH minigene does not impact on TIDA neuron excitability. **A**, pSTAT5 immunoreactivity illustrated via confocal Z-stack micrographs at low (10×) and high (63×) magnification in the dmArc of C57 WT (wt), DAT-tdTomato, and DAT-Cre mice injected with an hGH minigene-containing viral construct. **B**, Quantification of dopamine neurons per hemisphere/section (box plots in green and white, *N* = 8–12 per group, one-way ANOVA, *p* = 0.8881; Table 1), and dopamine neurons colocalizing with pSTAT5 (box plots in yellow, *N* = 8–12 per group, one-way ANOVA, *p* = 0.8059; Table 1). **C**, Representative traces of TIDA neuron firing patterns collected from C57 wt, DAT-tdTomato, and DAT-eYFP mice. **D**, Quantification of TIDA neuron firing frequency, recorded from the different mouse lines (*N* = 10–33 per group, one-way ANOVA, *p* = 0.7411; Table 1). Data are mean ± SEM. 3V, Third ventricle.

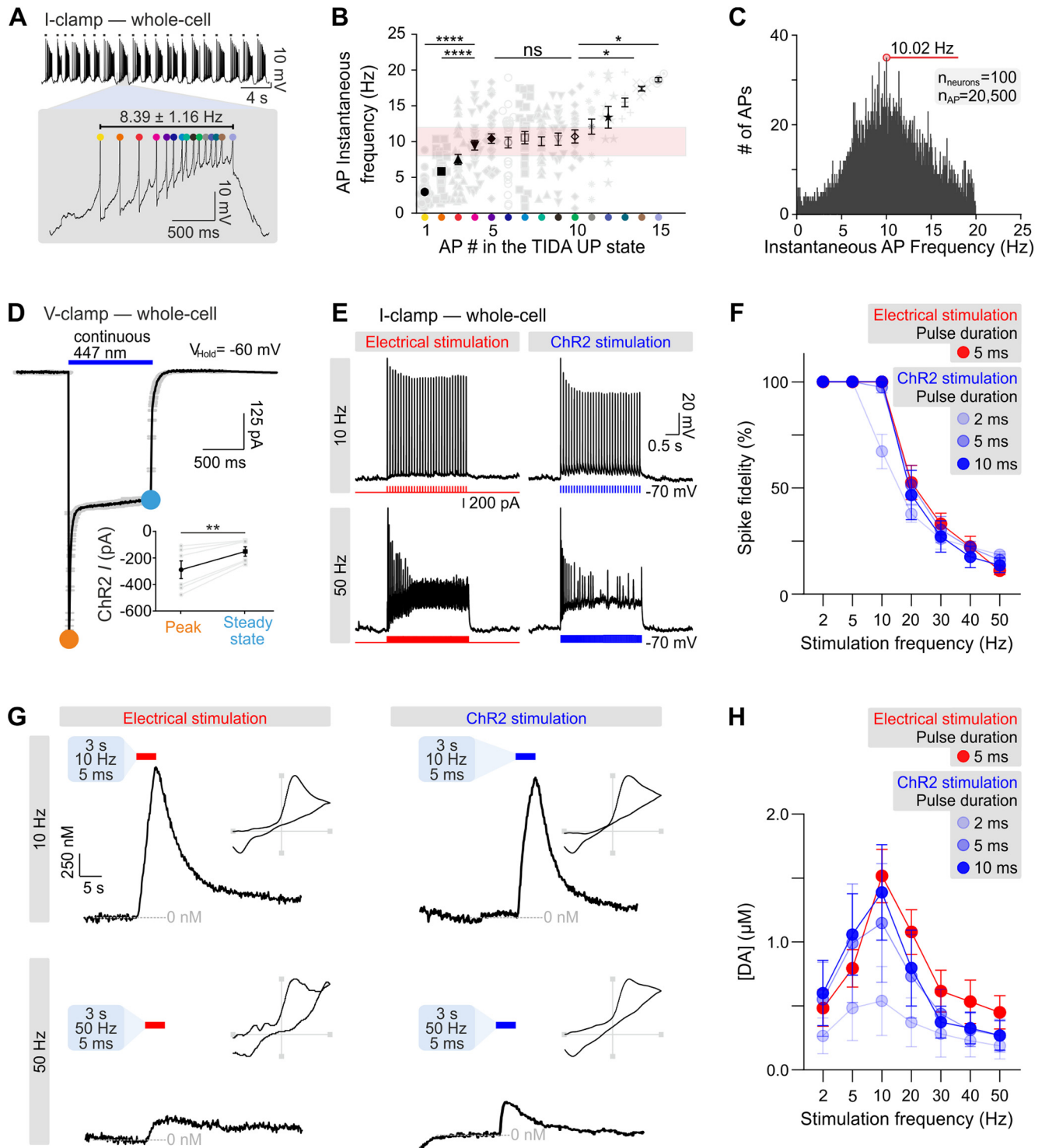


Figure 4. TIDA neuron endogenous firing frequency and optimal dopamine release in the ME terminals occur at 10 Hz. **A**, Whole-cell recording from a DAT-tdTomato neuron, with one UP state shown in expanded temporal resolution (gray box below; action potentials [AP] truncated for clarity). **B**, Quantification of the instantaneous firing frequency (IFF) of AP in an UP state ($N = 33$ cells, one-way ANOVA, $p < 0.0001$; Table 1). **C**, Frequency distribution of IFF shows that the majority of spikes are discharged at 10 Hz. **D**, ChR2 current at the peak and steady state, mediated via 1 s photostimulation ($N = 6$, two-tailed paired t test, $p = 0.0073$; Table 1). **E**, Representative traces with electrical square pulses and ChR2-driven AP firing at 10 and 50 Hz. The depolarization block and low fidelity are at 50 Hz. **F**, Quantification of spike fidelity versus photostimulation frequency and pulse width (repeated-measures one-way ANOVA; Table 1). **G**, Representative FSCV traces with electrically and ChR2-evoked dopamine release in the ME at 10 and 50 Hz. **H**, Quantification of dopamine release in the ME versus photostimulation frequency and pulse width (repeated-measures one-way ANOVA; Table 1). * $p < 0.05$, ** $p < 0.01$, *** $p < 0.001$, **** $p < 0.0001$. Data are mean \pm SEM.

(Fig. 2*G,H*; Table 1). Finally, coapplication of CdCl₂ (400 μ M) abolished the release of dopamine (Fig. 4*G,H*; Table 1). Together, these data suggest that dopamine release in the tuberoinfundibular pathway is both action potential- and Ca²⁺-dependent and thus relies on similar mechanisms as in other systems.

Frequency preference for maximal dopamine release at the level of the terminals matches the endogenous average firing frequency of TIDA neurons

The majority of action potentials in the UP states of spontaneously active TIDA neurons (Fig. 4*A*) are discharged within a \sim 10

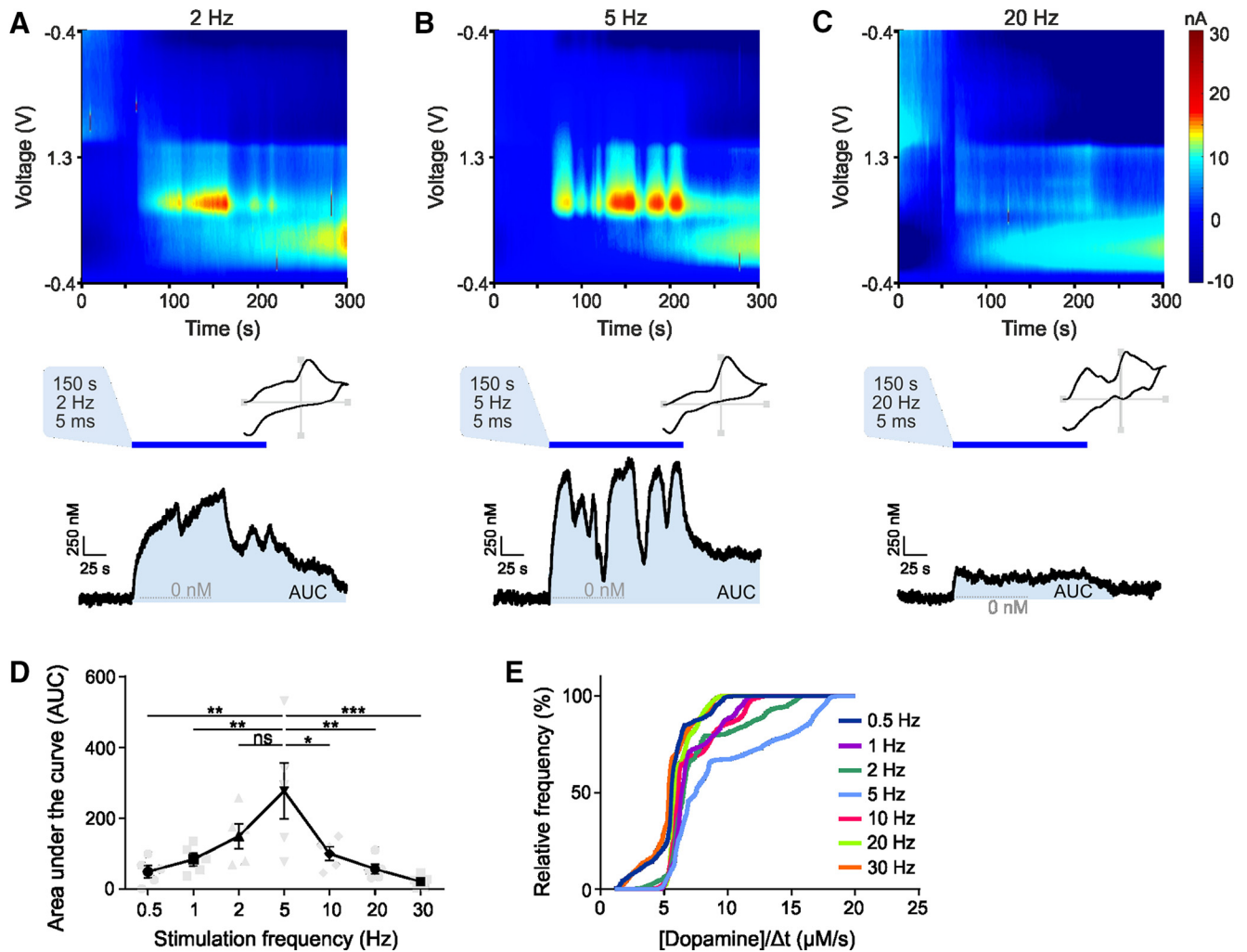


Figure 5. In tonic firing configuration, TIDA terminals release maximal amounts of dopamine in the ME at 5 Hz. **A–C**, Representative FSCV traces and heat maps with ChR2-evoked dopamine release in the ME at 2, 5, and 20 Hz. **D**, Quantification of dopamine release in the ME versus photostimulation frequency with 5 ms pulse width ($N = 5$, repeated-measures one-way ANOVA, $p = 0.0004$; Table 1). **E**, Relative frequency of dopamine release per second in the ME versus photostimulation frequency with 5 ms pulse width. * $p < 0.05$, ** $p < 0.01$, *** $p < 0.001$, **** $p < 0.0001$. Data are mean \pm SEM.

Hz frequency (Fig. 4B; $N = 33$, $F_{(14,338)} = 17.08$, $df = 14$, $p < 0.0001$, one-way ANOVA with Tukey’s test; Table 1), and the instantaneous frequency follows a normal-like distribution with a peak at 10.02 Hz (Fig. 4A, C). Following the characterization of the ChR2-mediated current with a fast and a slow component (Fig. 4D; $N = 6$, $t = 4.357$, $df = 5$, $p = 0.0073$, two-tailed paired t test; Table 1) in somatic recordings, we investigated the spike fidelity of the TIDA cells at different electrically and optically evoked stimulation frequencies. Electrical or optogenetic stimulation of DAT-Cre neurons at frequencies of ≤ 10 Hz yielded a 100% spike fidelity (Fig. 4E, top, F; Table 1), whereas higher photostimulation frequencies (30–50 Hz) led to a depolarization block phase with substantial spike failure (Fig. 4E, bottom, F; Table 1). The latter phenomenon has previously been described in rat TIDA cells in response to pharmacological manipulations (Stagkourakis et al., 2016).

Based on the observation that spontaneous TIDA discharge is strongly biased to the 10 Hz frequency band, we next addressed whether transmitter release at the TIDA terminals responds differentially at different stimulation frequencies. To investigate this issue, a brief (3 s) electrical or optical stimulation protocol was applied at frequencies ranging from 2 to 50 Hz. Electrically

evoked dopamine release was investigated in WT mice of C57BL/6J background, whereas optically evoked dopamine measurements were performed in ChR2 transduced DAT-Cre mice of the C57BL/6J background. Maximal dopamine release was recorded at 10 Hz using both methods of stimulation, with both higher and lower frequencies eliciting less dopamine signal (Fig. 4G, H). Importantly, the 10 Hz frequency yielded optimal dopamine release regardless of pulse duration when using a photostimulation protocol (Fig. 4H; Table 1). Together, these data suggest that the membrane properties of TIDA neurons, at the somatodendritic and axon terminal levels, are optimized to both discharge and release neurotransmitter content at 10 Hz.

As dopamine release dynamics may vary between short and long bouts of activity, we repeated the analysis of the frequency and pulse duration dependence of dopamine release using a longer-duration (150 s) photostimulation protocol. The maximal dopamine release signal was also here biased toward the slower frequencies, with the greatest value recorded at 5 Hz (Fig. 5A–E; Table 1). Interestingly, the average firing frequency of suprathreshold oscillating TIDA neurons recorded *in vitro* is detected in that range (Fig. 3C, D).

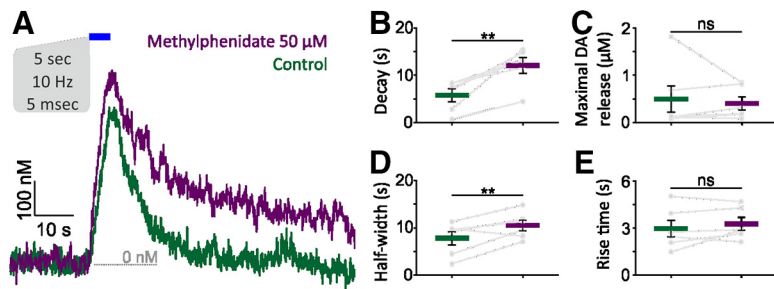


Figure 6. Dopamine release dynamics in the ME change upon DAT blockade. **A**, Representative dopamine-evoked oxidative current on baseline (green) and during (purple) DAT blockade with methylphenidate. **B–E**, Quantification of dopamine reuptake parameters, such as decay (**B**), maximal amplitude of dopamine release (**C**), half-width (**D**), and rise time (**E**) ($N = 6$, two-tailed paired t test; Table 1). * $p < 0.05$, ** $p < 0.01$, *** $p < 0.001$, **** $p < 0.0001$. Data are mean \pm SEM.

Functional DAT in the ME

The expression of DAT in TIDA neurons is well documented (Meister and Elde, 1993; Revay et al., 1996; Demaria et al., 2000; Stagkourakis et al., 2018), yet the functional role of the transporter within the lactotrophic axis remains controversial (Demarest and Moore, 1979; Annunziato et al., 1980; Meister and Elde, 1993; Revay et al., 1996; Bossé et al., 1997; Demaria et al., 2000; Stagkourakis et al., 2018). To assess whether reuptake is involved at determining dopamine levels at the entry to the portal vasculature, we performed optogenetic stimulation of TIDA terminals in the ME, in the absence and presence of the clinically prescribed DAT blocker, methylphenidate (Taylor and Ho, 1978; Volkow et al., 1999a, b). Following application of methylphenidate (10 μ M; Fig. 6A), the photostimulation-induced dopamine signal was augmented, quantified as prolonged decay (Fig. 6B; $N = 6$, $t = 4.439$, $df = 5$, $p = 0.0068$, two-tailed paired t test) and half-width (Fig. 6D; $N = 6$, $t = 5.228$, $df = 5$, $p = 0.0034$, two-tailed paired t test), whereas maximal [dopamine] release and rise time were not affected (Fig. 6C,D; Table 1). These data suggest the presence of functional dopamine transport active in the ME.

Capacity for dopamine release at the somatodendritic compartment of TIDA neurons

Recent work has suggested that local release of dopamine around the cell body and dendrites of TIDA neurons may serve as a critical component of an ultrashort feedback loop that tunes the electrical activity of these neurons to their recent transmitter secretion history (Belousov and van den Pol, 1997; Durham et al., 1998; Liang and Pan, 2012; Liang et al., 2014; Stagkourakis et al., 2016). Yet to date, no direct evidence exists that dopamine can indeed be released in the somatodendritic compartment in the dmArc. To investigate this possibility, TIDA cells were transduced with ChR2-eYFP. Inspection of cryostat sections of the dmArc of such animals revealed that the ChR2 construct was distributed on both cell bodies and dendrites of DAT-tdTomato-positive neurons (Fig. 7A). We next performed FSCV recordings in the dmArc with the carbon fiber electrode placed in the area occupied by TIDA cell somata (Fig. 7B). As in the ME, no spontaneous release could be recorded. When photostimulation was performed using the 5 s duration/10 Hz/5 ms pulse protocol found to evoke optimal release in the ME (Fig. 4H), however, a distinct dopamine signal could be recorded (Fig. 7C,D). This signal was typically 10- to 20-fold below that recorded in the ME (compare Fig. 7D and Fig. 4H). A photostimulation artifact is evident at ~ 0 and 1.3 V in the voltammogram, similar to what has been described previously (Bass et al., 2013). These results

provide strong evidence for a capacity for dopamine release at the cell body level of TIDA neurons.

Discussion

The ability of a neuron to translate electrical activity to chemical signal is a core feature of the nervous system. Studies of dopamine transmission in the basal ganglia (Oleson et al., 2009; L. Zhang et al., 2009; Bass et al., 2010; Sulzer et al., 2016) have identified several principles of stimulus-secretion coupling. Yet, the specific volume and coding mechanisms of release used by different brain systems are likely to vary depending on their role in behavior and physiology. Here we addressed this issue in the neuroendocrine tuberoinfundibular system, where

transmitter release from TIDA neurons can be monitored by FSCV while TIDA spiking patterns can be controlled by optogenetic stimulation.

We show that, while mouse TIDA neurons are able to spike across a spectrum of frequencies, in agreement with previous studies (Romanò et al., 2013; X. Zhang and van den Pol, 2015; Stagkourakis et al., 2018), action potentials are primarily discharged within a 10 Hz frequency band. When depolarized with greater stimulation than required to reach this frequency, TIDA neurons are successively more prone to depolarization block and spike failure (Stagkourakis et al., 2016; and present data). Importantly, maximal dopamine release was accomplished with a 10 Hz stimulation frequency (concomitant with full spike fidelity) and was abolished by the Na⁺ channel blocker TTX. Partial recovery was achieved via coapplication of TTX and the potassium channel blocker 4-AP (Petreanu et al., 2009), whereas coapplication of TTX, 4-AP, and the generic Ca²⁺ channel blocker CdCl₂ (Swandulla and Armstrong, 1989) abolished dopamine release at the TIDA terminals, suggesting that the dopamine thus recorded is the result of an action potential- and Ca²⁺-dependent process. Thus, the system appears to be operating at full capacity at its default spike rate (although it should be borne in mind that *in vivo* discharge frequencies, currently not known for the TIDA system, may be different). These results were recorded with 3 s stimulation bouts, in the range of the typical TIDA oscillation UP state in subthreshold oscillating cells (Stagkourakis et al., 2018). For extended periods (150 s) of stimulation, the optimal frequency was shifted toward slower frequencies. In the context of these findings, it can be noted that sustained (tonic) firing is triggered in TIDA neurons by modulators associated with inhibition of prolactin release upon central administration (Lyons et al., 2010; Briffaud et al., 2015). The firing frequency during this transmitter/hormone-induced persistent discharge can be lower than in the oscillatory state (Lyons et al., 2010), which may then offer an adaptation to the extended firing/lower frequency principle for optimal transmitter release suggested by the present data.

The dopamine concentration elicited by optogenetic stimulation ranged within ~ 0.5 – 1.5 μ M, comparable with the levels found in striatal recordings of dopamine release (Sulzer et al., 2016). The comparison between brain regions is fraught with complications, but it may be speculated that the dopamine concentrations evoked in the ME are likely diluted in the portal blood before reaching the target (lactotroph cells in the pituitary), unlike striatal dopamine concentrations, which potentially act di-

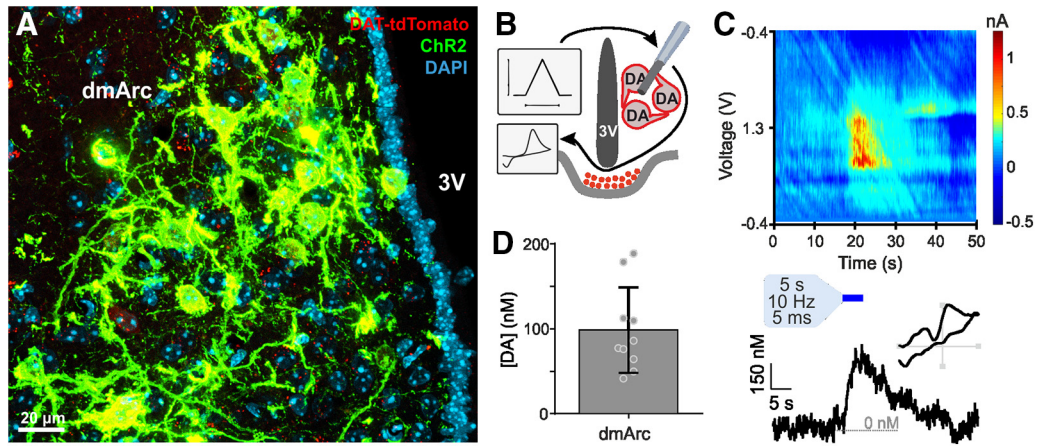


Figure 7. TIDA neurons release dopamine in the dmArc. **A**, Confocal Z-stack micrograph with virally mediated expression of Chr2-eYFP on DAT-tdTomato neurons in the dmArc. **B**, Experimental design of FSCV recordings aiming to record evoked dopamine release in dmArc. **C**, Representative FSCV trace with Chr2-evoked dopamine release in the dmArc. **D**, Quantification of evoked dopamine release in dmArc. Data are mean \pm SEM. 3V, Third ventricle.

rectly on the postsynaptic cells (Ross, 1991; Korchounov et al., 2010). But an additional possibility could be that excess dopamine is necessary to compensate for the relatively less precise delivery of dopamine across the neurovascular interface and capillary distribution system compared with the point-to-point synaptic transmission in the striatum. It can also be noted that the levels we recorded are several magnitudes above those required for activation of D2R autoreceptors (Gonon and Buda, 1985), which may be present on the somatodendritic compartments or TIDA terminals (Berry and Gudelsky, 1991; Huang et al., 2013; Stagkourakis et al., 2016).

Previous *in vitro* (Romanò et al., 2013) and *in vivo* (Romanò et al., 2017) amperometry investigations have indicated that increased firing (induced by prolactin administration) in the TIDA ensemble correlates to higher amperometric signal at the terminal level, and that a range of release even frequencies can be detected in the ME in the intact animal. Yet, a comprehensive understanding of the coupling between TIDA neuron activity and dopamine release at the terminals has been lacking. The superior ability of FSCV over amperometry to identify transmitters with chemical selectivity (Bucher and Wightman, 2015), combined with the millisecond precision control spiking through optogenetics, has allowed us in the current study to correlate specific firing patterns to dopamine release volumes in the TIDA system, without contamination of other transmitters and metabolites.

The role of DAT in TIDA neurons has been a subject of controversy. Pharmacological studies of dopamine accumulation initially suggested that dopamine reuptake had a minor effect on ME levels, leading to conclusions that a transporter system was not reconcilable with vascular release (Demarest and Moore, 1979; Annunziato et al., 1980). This conclusion has, however, been challenged by subsequent studies using other DAT antagonists (Demaria et al., 2000) and genetic deletion (Bossé et al., 1997). Indeed, a functional role for DAT in TIDA terminals received early support from the demonstration that the dopamine metabolite, 3,4-dihydroxyphenylacetic acid, likely the result of metabolism following reuptake, is a well-correlated surrogate marker for dopamine in the ME (Lookingland et al., 1987). Here, we show that optogenetically elicited dopamine release at the ME is powerfully amplified in the presence of methylphenidate, a clinically used antagonist of DAT. It is important to remember in this context that neuroendocrine neurons do not make immedi-

ate contact with portal capillaries, but rather abut a perivascular space (Ajika and Hökfelt, 1973) where release is postulated to occur. This organization suggests that secreted dopamine may linger for a period in the proximity of the terminal before ending up in the bloodstream, allowing for a window of opportunity for transmitter reuptake.

Recently, we have proposed the existence of an ultrashort D2R-mediated feedback loop (Stagkourakis et al., 2016). This model is primarily based on pharmacological and electrophysiological findings, but a key component of this scheme is the existence of release of ambient dopamine at the somatodendritic compartment, for which evidence has been lacking. The present study shows that release of dopamine can be triggered at the cell body level through optogenetic stimulation. Notably, the levels thus elicited were approximately a magnitude lower than what was recorded in the ME with similar stimulation. Our model proposes that local dmArc release mirrors fluctuations at the ME, but need not do so at similar absolute concentrations. Thus, the current findings support the existence of an autoinhibitory feedback loop. The exact release site for this evoked dopamine remains to be determined. Ultrastructural studies have demonstrated that TIDA neurons extend recurrent collaterals that project toward, but do not make direct contact with, TIDA cell bodies (Piotte et al., 1985), which could be providing extrasynaptic dopamine. There are, however, also dense dendrodendritic and somatodendritic contacts within the TIDA population (Piotte et al., 1985). In the midbrain, such contacts have been implicated in local release from the soma and/or dendrites (Hefti and Lichtensteiger, 1978; Cheramy et al., 1981; Rice and Patel, 2015). The current findings suggest that this possibility merits further investigation in the TIDA system.

In conclusion, the present data show how dopamine dynamics in the TIDA system correlate to spike rates, and identify regulatory mechanisms involved in this process at both the terminal and somatodendritic level. These findings offer insight into the relationship between electrical activity and signal substance release in the neuroendocrine system, and provide a platform for further investigations of stimulus-secretion coupling in the hypothalamo-pituitary axis.

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